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Analytical Modelling and Simulation of Single and Double Cone Pinholes for Real-Time In-Body Tracking of a HDR Brachytherapy Source

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Abstract—The choice of pinhole geometry is a critical factor in the performance of pinhole-collimator-based source tracking systems for brachytherapy QA. In this work, an analytical model describing the penetrative sensitivity of a single-cone pinhole collimator to photons emitted from a point source is derived. Using existing models for single-cone resolution and double-cone sensitivity and resolution, the theoretical sensitivity and resolution of the single-cone collimator are quantitatively compared with those of a double-cone collimator with an equivalent field of view. Monte Carlo simulations of the single and double-cone pinhole collimators using an accurate 3D model of a commercial high dose rate brachytherapy source are performed to evaluate the relative performance of each geometry for a novel real-time HDR brachytherapy QA system, HDR BrachyView. The theoretical penetrative sensitivity of the single-cone pinhole is shown to be higher than the double-cone pinhole, which is in agreement with the results from the Monte Carlo simulations. The wider pinhole response function of the single-cone collimator results in a larger total error between the projected centre of the source and the estimated centre of mass of the source projection for the single-cone collimator, with the greatest error (at the maximum FoV angle) being 0.54 mm for the double-cone pinhole and 1.37 mm for the single-cone at $\theta = 60^\circ$. The double-cone pinhole geometry is determined to be the most appropriate choice for the pinhole collimator in the HDR BrachyView probe.

Index Terms—Brachytherapy, source tracking, prostate cancer, analytical modelling, Monte Carlo simulations, pinhole collimators, imaging probe.

I. INTRODUCTION

Pinhole photon collimators are a critical element of many X-ray/gamma-ray imaging systems, and are found in applications ranging from diagnostic equipment such as high resolution single photon emission computed tomography (SPECT) cameras, to quality assurance (QA) systems for radioactive source tracking in brachytherapy [1, 2, 3, 4]. Accurate analytical modelling of the imaging properties of pinhole is essential for optimising the design of such collimators for their specific applications.

The two key metrics for pinhole collimator performance are spatial resolution and sensitivity [5, 6]. Spatial resolution quantifies the smallest spatial feature which can be resolved using a given imaging system, while the sensitivity of a pinhole camera is defined as the fraction of photons emitted by

the source which reach the imaging plane. Pinhole sensitivity includes two components: a geometric term, which accounts for the photons that pass directly through the physical aperture and are not subject to attenuation, and a penetration term, which accounts for the photons that pass through the attenuating medium from which the collimator is fabricated.

Several models have previously been proposed for a variety of pinhole types and imaging applications.

Jansen et al. introduced a geometric model for multiple keel-edge pinhole collimators in a conventional gamma camera system [7]. The model is used to solve the problem of overlapping projections and to jointly optimise the sensitivity and resolution.

Accorsi and Metzler have previously described an analytical model for the spatial resolution and sensitivity of a double-cone pinhole design [5, 6]. The derived pinhole resolution model is known as the resolution equivalent effective diameter, d_{re} , and is defined as the diameter of an ideal pinhole fabricated from a perfectly radiation-opaque material which provides a geometric resolution equivalent to that of the real pinhole, but with a larger diameter that models the effects of photon penetration. The model for penetrative sensitivity is derived by determining the path length of incident photons emitted from an ideal point source (i.e. those photons which penetrate the surface of the collimator) and integrating the attenuated flux over all such points. It assumes that all photons with more than a certain angle of incidence are stopped within the collimator due to the thickness of material that they must traverse.

Huang et al. investigate analytical modelling of a finite aperture for small animal pinhole SPECT imaging [8]. The developed model describes the probability that a single photon emitted from the radiation source is detected on the imaging plane. The probability of photon detection is calculated based on the cross sectional intersection area from the source passing through the aperture and reaching the detector plane.

Bal and Acton derived an analytical model to characterise the sensitivity and resolution of a pinhole collimator [9]. The point spread function (PSF) was derived for two pinhole geometries: right-circular double-cone and oblique-circular double-cone. The methodology used to derive the pinhole sensitivity was the sum of the geometric and penetrative sensitivity components. The geometric part is determined based on the physical parameters of the pinholes. The penetrative term requires calculating the path length of photons

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89 passing through the pinhole material subject to attenuation
 90 and exiting out the end of the aperture. It was demonstrated
 91 that for low to medium-energy photons, the PSF for the
 92 oblique-circular double-cone produced well-defined symmetric
 93 projections with the centre of mass of the projection closely
 94 correlated with the proper geometric projection of the centre
 95 of the source. However, with higher-energy photons, the re-
 96 sulting PSF exhibited significant asymmetry. The right-circular
 97 double-cone geometry resulted in an asymmetric PSF for all
 98 photon energies. For a small aperture, the right circular double-
 99 geometry resulted in fewer penetrated photons and a more
 100 compact PSF, making it ideal for high resolution imaging
 101 systems. However, the study does not extend the model to
 102 a include single-cone geometries, which is a common pinhole
 103 model used in imaging systems.

104 In this paper, the analytic model for the sensitivity of a
 105 double-cone collimator (originally introduced by Metzler et al.
 106 [6]) is extended to a single-cone pinhole geometry. The model
 107 is validated against Monte Carlo simulations and used to
 108 determine the optimal choice of pinhole design for a collimator
 109 to be used in a novel QA system for high dose rate (HDR)
 110 prostate brachytherapy.

111 The extension to the analytical sensitivity model of Metzler
 112 et al. is derived in Section II. The system for which the models
 113 have been developed, High Dose Rate (HDR) *BrachyView*, is
 114 a recently-proposed QA system for real-time in-body imaging
 115 of an HDR prostate brachytherapy source. The design and
 116 source localisation method together with the simulated and
 117 experimental characterisation of the device have been previ-
 118 ously reported [3, 10, 11]. In brief, the device is composed of
 119 a tungsten pinhole collimator and an array of high-resolution
 120 silicon photodetectors enclosed within a transrectal probe.
 121 Images of the source are projected through each pinhole onto
 122 the detector plane, automatically segmented, and the centres
 123 of mass of the projections are back-projected through the
 124 corresponding pinholes. An estimate of the three-dimensional
 125 source position is determined by finding the point in space with
 126 minimum mean squared distance to all of the backprojected
 127 rays. As there are seven pinholes, a unique solution exists
 128 provided that at least two projections are visible; however,
 129 the quality of the estimate improves with the number of
 130 visible projections. The anatomical position of the source is
 131 found by co-registering the probe's coordinate system with the
 132 transrectal ultrasound (TRUS) system.

133 The probe is described in detail in Section II. The analytical
 134 predictions for spatial resolution and sensitivity for both single
 135 and equivalent double pinhole geometries are compared in
 136 Section III; the specific analytical results presented are based
 137 on a symmetric double-cone structure with a cylindrical con-
 138 necting channel as shown in Figure 1(a) and a single-cone
 139 structure with a wider full acceptance angle, again connected
 140 to the bottom of the collimator by a small cylindrical channel
 141 as shown in Figure 1(b).

142 Results from Monte Carlo simulations of *HDR BrachyView*
 143 with single and double pinhole collimators with the same
 144 geometry as the analytic comparison are presented in Section
 145 III. The analytic performance predictions for both designs are
 146 compared with the Monte Carlo simulation results in order to

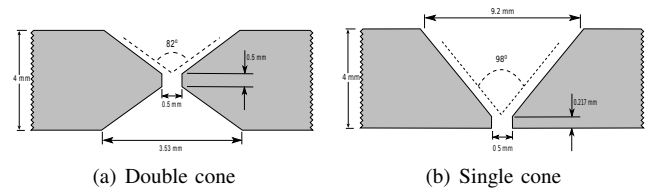


Fig. 1. Pinhole geometries proposed for the *HDR BrachyView* probe

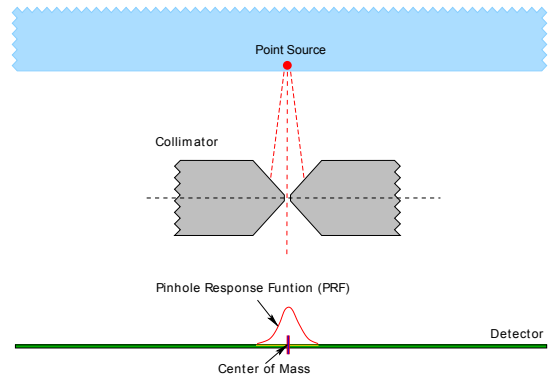


Fig. 2. The pinhole response function (PRF): distribution of photons on the imaging plane; its FwM is used as a measure of its resolution

147 determine the best pinhole geometry for *HDR BrachyView*.
 148 In Section IV, it is shown that the double-cone pinhole
 149 design provides a superior spatial resolution with an acceptable
 150 reduction in sensitivity, making it the preferred design for
 151 *HDR BrachyView*. Section V summarises our findings and
 152 describes the next steps in this project.

153 II. MATERIALS AND METHODS

154 A. Analytical Computation of Pinhole Resolution and Sensitivity

155
 156 The most important characteristics of a pinhole collimator
 157 are sensitivity and spatial resolution, both of which would be
 158 ideally as high as possible. However, there is an intrinsic trade-
 159 off between sensitivity and spatial resolution [2]. Increasing
 160 the acceptance angle of a pinhole collimator will increase the
 161 sensitivity to photon detection (and also the width of the field
 162 of view), but degrades the spatial resolution since the ratio of
 163 direct photons (photons that travel through the aperture of the
 164 pinhole) to penetrated photons (photons that penetrate through
 165 the tungsten collimator) decreases.

166 1) *Resolution*: Spatial resolution can be determined by
 167 finding the full width at k th maximum (FW k M) of the PSF or
 168 line spread function (LSF) of the imaging system. In the case
 169 of a pinhole camera, resolution is defined as the width of the
 170 pinhole response function (PRF) exceeding a fraction (k) of
 171 its maximum value (typically half, i.e. $k = 0.5$). The PRF is
 172 the 2D spatial distribution of the photons which are emitted
 173 by the point source, pass through the collimator and reach the
 174 imaging plane, as shown in Figure 2 [6, 12].

175 For an ideal pinhole with diameter d and a magnification
 176 factor M (defined as the ratio of projection size to the size
 177 of the original object), the resolution (λ) corresponding to the
 178 full width at half maximum (FWHM) is given by [13]:

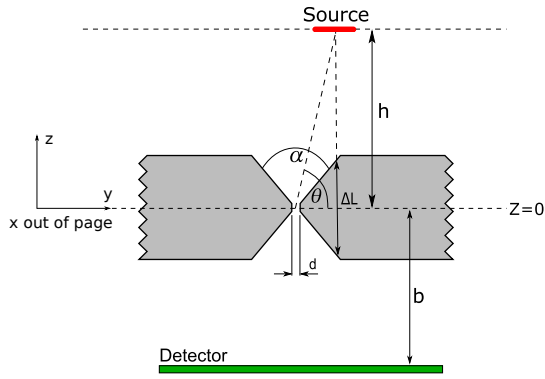


Fig. 3. Parameters of a pinhole collimator: The pinhole has a diameter d with a full acceptance angle α . A photon source, offset at angle θ to the y -axis at a distance h from the pinhole centre, projects onto the imaging plane. ΔL represents the path length of penetrated photons inside the collimator.

$$\lambda = d \left(1 + \frac{1}{M} \right) \quad (1)$$

179 A more general metric for quantifying pinhole resolution
 180 of a pinhole fabricated from a real material is the resolution
 181 equivalent effective diameter, d_{re} , which accounts for the
 182 angular offset of the point source with respect to the central
 183 axis of the pinhole [5, 6]. By definition, the PRF (and its
 184 corresponding $FWkM$) is directly proportional to its resolution
 185 equivalent diameter (d_{re}); that is, as d_{re} increases, pinhole
 186 resolution deteriorates (numerically increases, i.e. the PRF
 187 distribution broadens).

188 The parameters of the double-cone pinhole geometry are
 189 shown in Figure 3; parameter names are as for the single-
 190 cone pinhole geometry. ΔL represents the total distance inside
 191 the collimator traversed by penetrating photons before they
 192 are projected onto the imaging plane, i.e. the path length of
 193 photons that penetrate through the solid body of the collimator.

194 ΔL is a function of the polar radius ρ , and the azimuthal
 195 angle ϕ of the point source relative to the x -axis, shown in
 196 Figure 4(b). The figure shows the photons emitted by the point
 197 source (shown as the larger solid circle) passing through and
 198 leaving the collimator on the $z = 0$ plane (smaller solid circle).
 199 Due to azimuthal symmetry, ϕ may be assumed to be zero,
 200 which simplifies the problem without decreasing the generality
 201 of the result. The path length can be expressed as follows:

$$\Delta L = -\frac{\ln k}{\mu} \equiv \Delta L_k \quad (2)$$

202 where k determines the fraction value of the full width
 203 at k^{th} maximum of the PRF and μ is the linear attenuation
 204 coefficient of the medium.

205 2) *Sensitivity*: Pinhole sensitivity can be described mathe-
 206 matically as:

$$S_{total}(\theta) = S_{geom}(\theta) + S_{pen}(\theta) \quad (3)$$

207 where $S_{geom}(\theta)$ is the angle-dependent geometric sensi-
 208 tivity, which represents the fraction of incident photons that
 209 pass directly through the physical aperture and $S_{pen}(\theta)$ is the

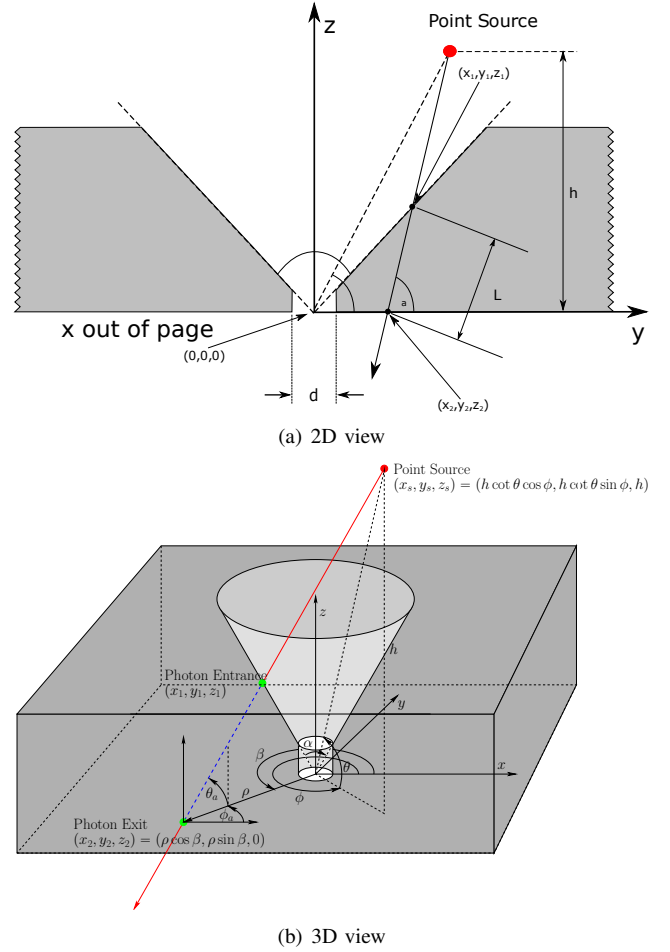


Fig. 4. Single cone pinhole collimator, showing all key geometric parameters

penetrative sensitivity, which represents the fraction of photons
 210 passing through the attenuating medium of the collimator. 211

The penetrative sensitivity for a double-cone pinhole colli-
 212 mator has been derived by Metzler et al. as follows [6]: 213

$$S_{pen}(\theta) \approx \frac{\sin^5 \theta \tan^2 \frac{\alpha}{2}}{8h^2 \mu^2} \times \left(1 - \frac{\cot^2 \theta}{\tan^2 \frac{\alpha}{2}} \right)^{1/2} \times \left[1 - \frac{\cot^2 \theta}{\tan^2 \frac{\alpha}{2}} + \mu d \csc \theta \cot \frac{\alpha}{2} \right] \quad (4)$$

214 An equivalent expression for penetrative sensitivity can be
 215 derived for a single-cone pinhole. $S_{pen}(\theta)$ is again dependent
 216 on the path length through the collimator's body. To calculate
 217 $S_{pen}(\theta)$, it is assumed that photons radiate from a point source
 218 in a spherical coordinate system. The path length of a photon
 219 penetrating the collimator at a fixed point is calculated. The
 220 path length is then calculated relative to the two points of
 221 intersection, (x_1, y_1, z_1) and (x_2, y_2, z_2) , shown in Figure 4(a),
 222 which is represented as (θ_a, ϕ_a) and parameterised relative to
 223 the reference frame of the origin $(x, y, z) = (0, 0, 0)$ repre-
 224 sented as (θ, ϕ) . The expression is then expanded, simplified
 225 and integrated using (5). The method adopted in this paper
 226 is similar to that derived by Metzler et al. for a double-cone

pinhole design [6]. A general expression for the penetrated photon sensitivity is given by

$$S_{pen}(\theta) = \frac{\sin^3 \theta}{4\pi h^2} \int_0^{2\pi} \int_{\frac{d}{2}}^{\infty} \rho e^{-\mu \Delta L} d\rho d\beta \quad (5)$$

where the integrand is the photon flux incident on the projection of an infinitesimal area $dA = \rho d\beta \cdot d\rho$ (on the $z = 0$ plane) onto a sphere of radius $h/\sin \theta$ originating at the point source, after attenuation through a section of material with linear attenuation μ of path length ΔL . The key problem is to determine an expression for the path length ΔL for a given cone geometry.

Figure 4(a) shows the Euclidean path length ΔL between the point of photon ingress and egress on the single-cone pinhole collimator in a spherical coordinate system, assuming the point source to be within the extended projection of the cone (if a source is outside this region, the pinhole can be ignored as any penetrating photons will traverse at least the total thickness of the collimator plate, with a very high probability of absorption).

The points shown in (6) and (7) represent the upper and lower points of intersection respectively between a penetrating photon's trajectory and the body of the collimator. Equation (8) is the formula of a cone; hence the expressions for x_1 and y_1 in terms of z_1 may be substituted for x and y in (8) and rearranged to yield a quadratic equation in terms of z_1 , which can be solved to yield two solutions.

$$(x_1, y_1, z_1) = (\rho \cos \beta + z_1 \cot \theta_a \cos \phi_a, \rho \sin \beta + z_1 \cot \theta_a \sin \phi_a, z_1) \quad (6)$$

$$(x_2, y_2, z_2) = (\rho \cos \beta, \rho \sin \beta, 0) \quad (7)$$

$$x^2 + y^2 = \left(z \tan \frac{\alpha}{2} \pm \frac{d}{2} \right)^2 \quad (8)$$

To simplify the analysis, it is assumed that $d = 0$. This does not significantly affect the penetrated photon distribution as the maximum thickness of the collimator is only 0.2 mm at the point where the channel is drilled, so attenuation of photons in this region is negligible. The expression for z_1 with $d = 0$ yields:

$$z_1 = \frac{-\rho \cos(\beta - \phi_a) \cot \theta_a + \sqrt{\rho^2 \cos^2(\beta - \phi_a) \cot^2 \theta_a - \rho^2 \cot^2 \theta_a + \rho^2 \tan^2 \frac{\alpha}{2}}}{\cot^2 \theta_a - \tan^2 \frac{\alpha}{2}} \quad (9)$$

Now, calculating the Euclidean distance between the two points of intersection (x_1, y_1, z_1) and (x_2, y_2, z_2) to find ΔL :

$$\Delta L^2 = z_1^2 \cot^2 \theta_a \cos^2 \phi_a + z_1^2 \cot^2 \theta_a \sin^2 \phi_a + z_1^2 \quad (10)$$

Substitution of (9) into (10) yields an expression for ΔL :

$$\Delta L = \frac{\rho \csc \theta_a \left(\sqrt{\tan^2 \frac{\alpha}{2} - \cot^2 \theta_a \sin^2(\beta - \phi_a)} - \cot \theta_a \cos(\beta - \phi_a) \right)}{\cot^2 \theta_a - \tan^2 \frac{\alpha}{2}} \quad (11)$$

The path length needs to be expressed in terms of θ and ϕ , the elevation and azimuth of the point source relative to the aperture. Equation (11) is then expressed in terms of absolute source elevation and azimuth angles (θ, ϕ) using the same trigonometric relations used by Metzler et al. [6]; due to azimuthal symmetry, ϕ may be assumed to be zero, resulting in (12):

$$\Delta L = \frac{\sqrt{\frac{\rho^2}{h^2} - 2\frac{\rho}{h} \cos \beta \cot \theta + \csc^2 \theta}}{-(\tan^2 \frac{\alpha}{2} - \frac{\rho^2}{h^2} + 2\frac{\rho}{h} \cos \beta \cot \theta - \cot^2 \theta)} \times \left[\rho \sqrt{\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta} - \rho \cos \beta \cot \theta + \frac{\rho^2}{h} \right] \quad (12)$$

Since $\rho \ll h$ (as it is assumed that the point source is inside the projection of the pinhole cone), we can use the approximation $\frac{\rho^2}{h^2} \approx 0$. The numerator and denominator of (12) are then expanded in terms of $\frac{\rho}{h}$, resulting in (13):

$$\begin{aligned} \Delta L &\approx \frac{\csc \theta \left(1 - \frac{\rho}{h} \cos \beta \sin \theta \cos \theta \right)}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \times \\ &\frac{\sqrt{\rho^2 \tan^2 \frac{\alpha}{2} - \rho^2 \sin^2 \beta \cot^2 \theta} - \rho \cos \beta \cot \theta + \frac{\rho^2}{h}}{2\frac{\rho}{h} \frac{\cos \beta \cot \theta}{\tan^2 \frac{\alpha}{2} - \cot^2 \theta} + 1} \\ &= \frac{\csc \theta \left(1 - \frac{\rho}{h} \cos \beta \sin \theta \cos \theta \right) \left(1 - 2\frac{\rho}{h} \frac{\cos \beta \cot \theta}{\tan^2 \frac{\alpha}{2} - \cot^2 \theta} \right)}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \times \\ &\left(\sqrt{\rho^2 \tan^2 \frac{\alpha}{2} - \rho^2 \sin^2 \beta \cot^2 \theta} - \rho \cos \beta \cot \theta + \frac{\rho^2}{h} \right) \\ &= \frac{\csc \theta \left(1 - 2\frac{\rho}{h} \frac{\cos \beta \cot \theta}{\tan^2 \frac{\alpha}{2} - \cot^2 \theta} - \frac{\rho}{h} \cos \beta \sin \theta \cos \theta \right)}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \times \\ &\left(\sqrt{\rho^2 \tan^2 \frac{\alpha}{2} - \rho^2 \sin^2 \beta \cot^2 \theta} - \rho \cos \beta \cot \theta + \frac{\rho^2}{h} \right) \quad (13) \end{aligned}$$

Expanding (13) and assuming all second order $\frac{\rho^2}{h^2}$ terms to be negligible, results in the following approximation for ΔL :

$$\Delta L \approx \frac{\rho \csc \theta \left(\sqrt{\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta} - \cos \beta \cot \theta \right)}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \times \left(-2\frac{\rho}{h} \frac{\cos \beta \cot \theta}{\tan^2 \frac{\alpha}{2} - \cot^2 \theta} - \frac{\rho}{h} \cos \beta \sin \theta \cos \theta + 1 \right) \quad (14)$$

Since $\int_0^{2\pi} \cos \beta d\beta = 0$, each of the terms in (14) with a $\cos \beta$ factor will become zero after integration with respect to β . Equation (14) therefore reduces to:

$$\Delta L \approx \frac{\rho \csc \theta \sqrt{\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta}}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \quad (15)$$

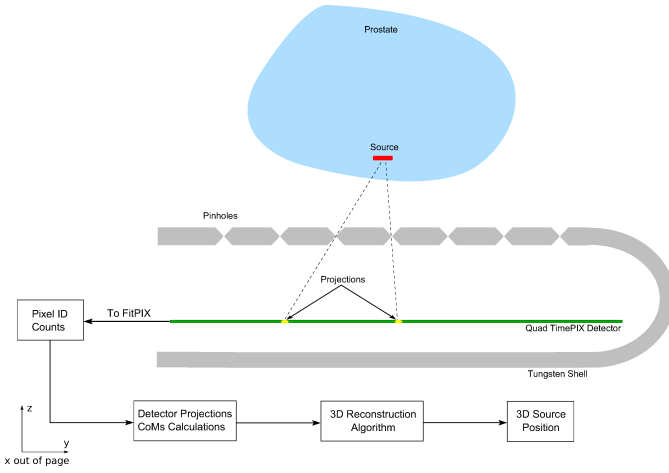


Fig. 5. Conceptual diagram of HDR BrachyView imaging system.

(15) can now be integrated using (5).

$$\begin{aligned}
 S_{pen}(\theta) &\approx \frac{\sin^3 \theta}{4\pi h^2} \int_0^{2\pi} d\beta \times \\
 &\int_0^\infty \rho \exp \left[-\mu \frac{\rho \csc \theta \sqrt{\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta}}{\cot^2 \theta - \tan^2 \frac{\alpha}{2}} \right] d\rho \\
 &\approx \frac{\sin^3 \theta}{4\pi h^2} \left[\frac{\sec^4 \frac{\alpha}{2} \csc^2 \theta (\cos \alpha + \cos 2\theta)^2}{4\mu^2 (\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta)} \right] \int_0^{2\pi} d\beta
 \end{aligned} \quad (16)$$

Finally, integrating with respect to β results in an approximate expression for the sensitivity due to penetration for a single-cone pinhole collimator (17):

$$\begin{aligned}
 S_{pen}(\theta) &\approx \frac{\sin^3 \theta}{8\pi h^2 \mu^2} \sec^4 \frac{\alpha}{2} \csc^2 \theta (\cos \alpha + \cos 2\theta)^2 \times \\
 &\int_0^{2\pi} \frac{d\beta}{\tan^2 \frac{\alpha}{2} - \sin^2 \beta \cot^2 \theta} \\
 &= \frac{\tan^2 \frac{\alpha}{2} \sin^5 \theta}{4\sqrt{2} h^2 \mu^2} \left[-\csc^2 \frac{\alpha}{2} \csc^2 \theta (\cos \alpha + \cos 2\theta) \right]^{3/2}
 \end{aligned} \quad (17)$$

B. The HDR BrachyView Real-time QA Imaging System

A novel real-time QA system for real-time in-body tracking of a HDR prostate brachytherapy source, HDR BrachyView, is currently under development at the University of Wollongong Center for Medical Radiation Physics (CMRP) in parallel with a related low dose rate (LDR) version [3, 4, 11]. This transrectal source-monitoring system for HDR brachytherapy uses projections of the source through multiple pinholes in a tungsten collimator onto a pixelated silicon detector to track the source position in real time. The centres of mass (CoMs) for each projection are then located, and a line from each of the CoMs is backprojected through the corresponding pinhole collimator. The source location is found by finding the point in space with the minimum mean squared distance

to all back-projected lines. The imaging area consists of four TimePix detectors, each with an individual sensitive area of 15 mm × 15 mm divided into an array of 256 × 256 pixels [14, 15]. The total imaging area that will be used as the rectal probe is 15 mm × 56 mm with a total of 256 × 1024 pixels. The system needs to be able to track and image an ^{192}Ir source anywhere within the nominal prostate volume of 40 × 40 × 40 mm³ shown in Figure 5. In HDR BrachyView, the distance between the probe and the source may be as little as 5 mm; additionally, the mean energy of the ^{192}Ir source is 380 keV, which is highly penetrating. Consequently, the collimator needs to provide as much attenuation as possible; however, due to space constraints inside the HDR BrachyView probe, the maximum feasible thickness is 4 mm. A commercially available tungsten alloy (95% W, 3.5% Ni and 1.5% Cu) was chosen as the material for the collimator, since a 4 mm thick collimator fabricated from this alloy blocks approximately 80% of incident 380 keV photons.

The collimator used in the QA probe employs conical pinholes with a truncated knife-edge geometry. Two alternative pinhole geometries were investigated: the first is a symmetric double-cone design, where the cones are connected by a small cylindrical channel; the second uses a single cone with a wider acceptance angle connected to the bottom face by a small cylindrical channel as. The double and single cone pinholes are shown in Figures 1(a) and 1(b), respectively. Both pinhole designs have a connecting channel diameter of $d = 0.5$ mm. The acceptance angles (α) for the double and single-cone pinholes were set to 82° and 98° respectively; these angles allow the entire sensitive surface of the detector array to be used, given the geometric constraints of the rectal probe, and provide good visibility to more than 70% of the prostate volume. The remaining regions (at the bottom of the prostate volume on either side of the y axis) can be monitored (if necessary) by rotating the probe either clockwise or anticlockwise. The acceptance angles were calculated by projecting lines from the corners of the detector through the collimator at the base of the pinhole channel. The acceptance angle is calculated using (18), where b is the distance between the pinhole and detector and x is the distance between the centre of pinhole on the detector plane and the edge of the detector.

$$\alpha = 2 \tan^{-1} \left(\frac{x}{b} \right) \quad (18)$$

d_{re} for the double-cone (d_{re}^{dc}) and single-cone (d_{re}^{sc}) pinholes are given by the respective approximations:

$$d_{re}^{dc} \approx d - \frac{\ln k}{\mu} \left(\tan^2 \frac{\alpha}{2} - \cot^2 \theta \right) \cot \frac{\alpha}{2} \sin \theta \quad (19)$$

$$d_{re}^{sc} \approx d - 2 \frac{\ln k}{\mu} \sin \theta \tan \frac{\alpha}{2} \quad (20)$$

C. Monte Carlo Simulations

Monte Carlo simulations of the double-cone and single-cone pinhole geometries were performed, based on the design of the HDR BrachyView system described in Section II-B. A

342 tungsten alloy plate with conical pinholes and an ^{192}Ir source
 343 were modelled in Geant4. The simulated source consists of
 344 a core made from an alloy of 10% ^{192}Ir and 90% platinum
 345 surrounded by a pure platinum shell; this structure is based
 346 on Alpha-Omega Services HDR ^{192}Ir source [16]. A pixelated
 347 silicon detector was placed 8.5 mm below the centre of the
 348 collimator. The source-to-pinhole height h for the double-cone
 349 and single-cone were set as 7 mm and 9 mm respectively. h
 350 is 2 mm greater for the single-cone pinhole simulation since
 351 the centre of the pinhole is shifted 2 mm lower compared to
 352 the double-cone pinhole.

353 Figure 6 shows the geometry of both the double-cone and
 354 single-cone simulations. Five source positions were simulated
 355 for each pinhole geometry, with the centre of the source
 356 located at $(\theta, \phi) = (60^\circ, 0^\circ)$, $(60^\circ, 90^\circ)$, $(75^\circ, 0^\circ)$, $(75^\circ, 90^\circ)$
 357 and $(90^\circ, 0^\circ)$. The cases where $\theta = 60^\circ$ represent the most
 358 extreme location of the source, where it is placed at the very
 359 edge of the pinhole FoV; $\theta = 90^\circ$ represents the best-case
 360 scenario where the source is directly above the pinholes and
 361 $\theta = 75^\circ$ is an intermediate value. For $\phi = 0$, the source
 362 is translated in a direction parallel to its major axis (that is,
 363 along the y -axis); for $\phi = 90^\circ$, the source is moved in a
 364 direction perpendicular to its major axis (that is, along the
 365 x -axis). Four billion photon events were generated for each
 366 simulation; the photon energy distribution was generated based
 367 on the standard ^{192}Ir spectrum [16].

368 Monte Carlo simulations were performed to validate the
 369 analytical sensitivity models. The simulation scenario was
 370 configured similarly to the previous simulations, with two
 371 simplifications to match the assumptions used in the analytic
 372 model: firstly, the geometry of the pinholes was changed to a
 373 knife-edge design (i.e. the cylindrical channel was removed),
 374 and secondly, the HDR source was changed to a point source.
 375 The same source positions were simulated. The analytical
 376 models were reintegrated using (5) with a finite value of ρ
 377 to ensure that the RoI was within the detector FoV in the
 378 simulation.

379 III. RESULTS

380 A. Analytical Computation of Pinhole Resolution and Sensitivity

381
 382 1) *Resolution*: Using (19) and (20), the resolution equivalent
 383 diameter d_{re} for both double and single-cone pinholes was
 384 analytically determined for values of k between 0.1 and 1. The
 385 following parameters (as illustrated in Figure 1(a) and 1(b))
 386 were used for both the double-cone and single-cone pinholes
 387 to analytically determine values of d_{re}^{DKKE} and d_{re}^{SKE} . The
 388 analytical values of d_{re} were used to calculate the theoretical
 389 FWHM of the projections at the detector plane for both single-
 390 cone and double-cone pinhole geometries and were compared
 391 to the FWHMs of the projected images obtained from the
 392 simulation.

393 The linear attenuation coefficient (μ) was assumed to be
 394 approximately $5.2 \pm 0.1 \text{ cm}^{-1}$ for tungsten at 380 keV. d_{re}
 395 was determined at the three source angles chosen from the
 396 Monte Carlo simulations, 60° , 75° and 90° , for both pinhole
 397 geometries.

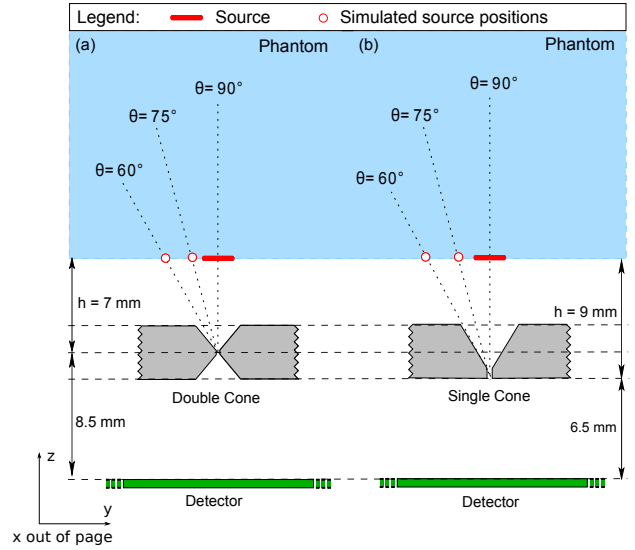


Fig. 6. The simulated positions of the source, collimator, phantom and detector for the double-cone pinhole (a) and the single-cone pinhole (b). The illustration shows the source being translated along the y -axis (i.e. $\phi = 0^\circ$); a similar translation is separately performed along the x -axis ($\phi = 90^\circ$), for a total of 5 source positions (at the same vertical distance above the collimator and detector).

398 Graphs showing the analytical estimates of resolution-
 399 equivalent diameter for both double-cone and single-cone
 400 pinhole geometry are shown in Figure 7.

401 2) *Sensitivity*: Analytical expressions for double-cone and
 402 single-cone pinhole sensitivity ((4) and (17) respectively)
 403 are normalised to their respective source-to-collimator dis-
 404 tance (h_{DKKE} , h_{SKE}) and plotted as functions of horizontal
 405 source displacement y with vertical source-to-pinhole dis-
 406 tances $h_{DKKE} = 7, 23, 43 \text{ mm}$ (or $h_{SKE} = 9, 25, 45 \text{ mm}$
 407 for the single cone geometry) as shown in Figures 8(a), 8(b)
 408 and 8(c), respectively.

409 B. Monte Carlo Simulation

410 Images of the ^{192}Ir source model projected through the
 411 simulated double-cone and single-cone pinhole collimators,
 412 generated using 4 billion photon events, are shown in Figure 9.
 413 Each figure illustrates the projection of the HDR source onto
 414 a single 256×256 pixel detector array. The source was
 415 simulated at the five locations $(\theta, \phi) = (60^\circ, 0^\circ)$, $(60^\circ, 90^\circ)$,
 416 $(75^\circ, 0^\circ)$, $(75^\circ, 90^\circ)$ and $(90^\circ, 0^\circ)$ for both pinhole geome-
 417 tries. One-dimensional image profiles were obtained across the
 418 centre of the projection (along the x -axis). As the underlying
 419 function is known to be smooth and continuous, a Savitsky-
 420 Golay filter was applied to the profiles to reduce noise and
 421 smooth the profile without distorting its underlying shape; the
 422 original and smoothed signals are shown in Figure 10.

423 The full width at k^{th} maximum of the smoothed PRFs were
 424 measured directly. The $\text{FW}k\text{M}$ was then plotted against each
 425 value of k for the double-cone and single-cone pinhole for
 426 three values of θ as shown in Figure 11.

427 Figures 12(a) and 12(b) display the analytical and simulated
 428 penetrative sensitivity of the double and single-cone pinholes,
 429 respectively. The analytical models were integrated using a

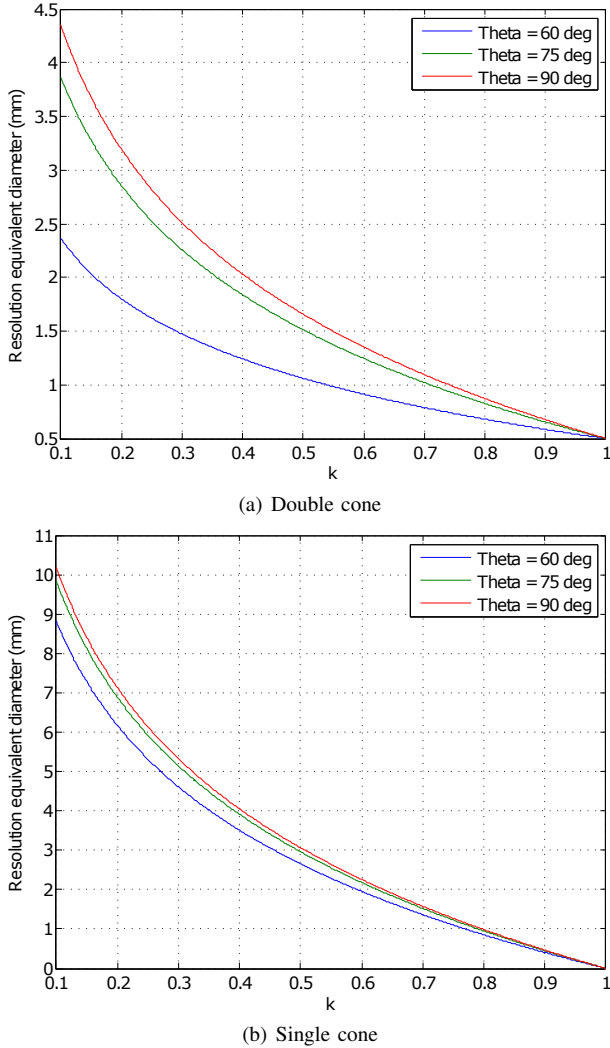


Fig. 7. Analytical estimate of the resolution-equivalent diameters d_{re}^{DKE} and d_{re}^{SKE} for double and single-cone pinholes, respectively. The full widths at k th maximum are shown for k between 0.1 and 1, for source positions $\theta = 90^\circ$, 75° and 60° ($\phi = 0^\circ$).

finite value of ρ as the upper limit. This value was calculated to achieve a RoI covering the detector plane once integrated over the azimuthal angle. The same RoI was used for both geometries. The sensitivity from the simulations was then calculated by integrating over the same RoI on the detector plane. Both data sets were normalised at $\theta = 90^\circ$. The confidence intervals in the simulations represent $\pm 3\sigma$ (99.7% confidence).

IV. DISCUSSION

A. Analytical Calculations

From Figure 7, it may be observed that d_{re} for the double-cone pinhole is consistently smaller than the value for the single-cone pinhole for each case of $\theta = 90^\circ$, 75° and 60° . Therefore, it is concluded that, in general, the double-cone pinhole geometry has a narrower PRF and hence will block a larger fraction of high-energy photons close to the aperture compared to an equivalent single-pinhole geometry. The FWHM ($k = 0.5$) for the double-cone has a d_{re} of 1.7 mm

compared with the FWHM of the single-cone with a d_{re} value of 3.10 mm at $\theta = 90^\circ$. For both designs, when the source is placed directly above the collimator (i.e. $\theta = 90^\circ$), d_{re} is at its maximum. This is due to the large photon flux in the neighbourhood of the aperture and hence higher photon penetration through the collimator around the pinhole. This broadens the PRF and degrades the spatial resolution. As the source moves away from the pinhole i.e. at $\theta = 75^\circ$ and $\theta = 60^\circ$, fewer photons penetrate around the aperture of the pinhole, creating a slightly narrower PRF and improving the spatial resolution.

Figures 8, shows the theoretical penetrative sensitivity for the double-cone and single-cone pinhole geometries as a function of horizontal source displacement in the y direction (moving towards the edge of the FoV as y increases). The penetrative sensitivity term was derived analytically by assuming the path length of incident photons through the collimator are as for an ideal point source; however, the source used in HDR BrachyView has a physical length of 3 mm and therefore cannot be accurately modelled as a point source, particularly when the source is close to the collimator. Sensitivity varies across the length of the source, and hence the relative sensitivity is much greater for the single-cone compared with the double-cone pinhole because the sensitivity of the double-cone decreases more rapidly with horizontal displacement compared to the single-cone geometry.

B. Monte Carlo Simulation

The projection images from the simulated double-cone pinhole collimator exhibit a much sharper image of the source compared with the single-cone pinhole collimator, confirming the predicted analytical results for pinhole resolution. There is also less penetration close to the aperture of the double-cone pinhole compared with the single-cone case. The total number of photons for a given source activity and exposure time is greater with the single-cone pinhole geometry, therefore its sensitivity is better than the double-cone pinhole.

As the source moves away from the centre of the pinholes, the CoM of the projection shifts in the direction of the pinhole relative to the projected centre of the source (the point of intersection of the line drawn between the source centre and the pinhole apex with the detector plane). The differences between the CoMs of the projections and the projected source centres are summarised in Tables I and II for double-cone and single-cone pinholes, respectively. The shift increases for both pinholes as θ increases, since the source is not a point source; rather, it has a physical length of 3.6 mm and a width of 0.65 mm. This means that the end or side of the source that is closest to the pinhole contributes in a greater photon flux density on the imaging plane compared to the far end of the source. At $\theta = 60^\circ$, the centre of the source is at the very edge of the FoV, which means that part of the source is actually outside the FoV (either one end of the source, for $\phi = 0^\circ$, or both ends of the source, for $\phi = 90^\circ$). This is the main reason for the significantly higher shift relative to projected centre of source which is observed for both collimators at $(\theta, \phi) = (60^\circ, 90^\circ)$; however, the error is much greater for the

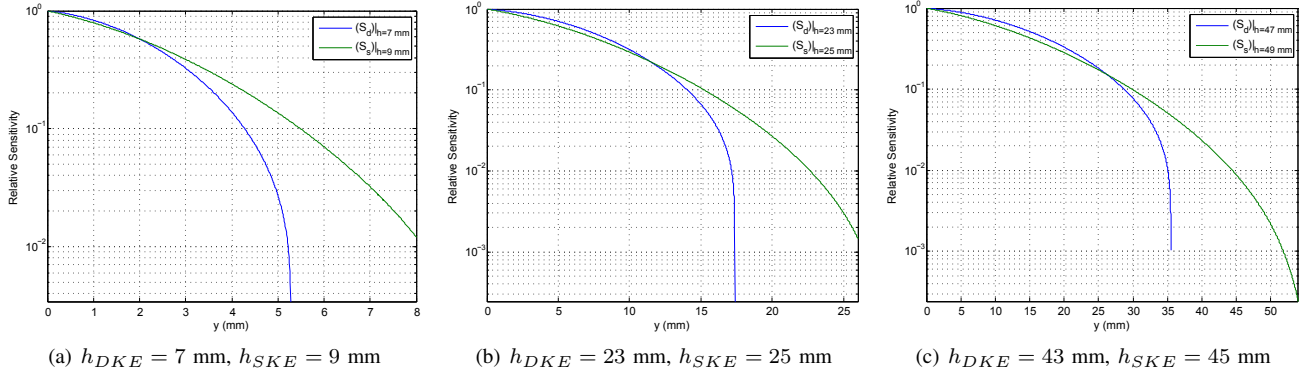


Fig. 8. Analytical expressions for the penetrative sensitivity for double-cone and single-cone pinholes at various source-to-collimator distances, normalised to their respective source-to-collimator distance (h_{DKE} , h_{SKE}) and plotted against horizontal source displacement y , where $y = 0$ is the position directly above the centre of the pinhole.

TABLE I

LOCATION OF THE CENTRE OF THE SOURCE PROJECTED THROUGH THE CENTRE OF THE DOUBLE-CONE PINHOLE COMPARED TO THE LOCATION OF THE CENTRE OF MASS OF THE PROJECTED IMAGE.

Source position (θ , ϕ)	Analytic		Simulation		Error		
	x (mm)	y (mm)	x (mm)	y (mm)	Δx (mm)	Δy (mm)	Δd (mm)
90° , 0°	0	0	0.136	0.0285	0.136	0.0285	0.139
75° , 0°	0	2.28	0.00580	1.50	0.00580	0.776	0.776
60° , 0°	0	4.91	0.0900	3.44	0.09	1.47	1.47
75° , 90°	2.28	0	1.99	0.499	0.292	0.499	0.579
60° , 90°	4.91	0	4.38	0.127	0.529	0.127	0.544

TABLE II

LOCATION OF THE CENTRE OF THE SOURCE PROJECTED THROUGH THE CENTRE OF THE SINGLE-CONE PINHOLE COMPARED TO THE LOCATION OF THE CENTRE OF MASS OF THE PROJECTED IMAGE.

Source position (θ , ϕ)	Analytic		Simulation		Error		
	x (mm)	y (mm)	x (mm)	y (mm)	Δx (mm)	Δy (mm)	Δd (mm)
90° , 0°	0	0	0.128	0.0221	0.127	0.0221	0.130
75° , 0°	0	1.74	0.0545	1.10	0.0545	0.642	0.644
60° , 0°	0	3.75	0.120	2.33	0.09	1.42	1.43
75° , 90°	1.74	0	1.24	0.0442	0.500	0.0442	0.502
60° , 90°	3.75	0	2.41	0.226	1.35	0.226	1.37

single-cone case, since the difference in thickness of tungsten traversed by the out-of-FoV portion of the source on either side of the pinhole is greater than for the double-cone case. Therefore, the CoM of the projection at $(\theta, \phi) = (60^\circ, 90^\circ)$ is a better estimate of the projected centre of the source for the double-cone pinhole.

A smaller effect is also evident when the source is entirely within the FoV due to the differential free-space path length traversed by photons emitted from each end or each side of the source and passing directly through the pinhole aperture. This differential path length results in a differential photon flux at the two ends of the projection, causing its CoM to shift closer to the pinhole and introducing a small systematic error in the same direction as the source displacement. For both pinhole collimators, when $\theta = 90^\circ$, the projected source centre and the CoM of the source projection are both directly below the pinhole. As the source is translated along the y -axis or x -axis, the difference in location of the projected source centre and the CoM of the simulated source projection increases by similar

amounts for both pinhole collimators.

Figure 11 shows how the FWHM changes for different values of θ and confirms that the resolution of the double-cone pinhole geometry is also superior to that of the single-cone pinhole, as predicted by the analytical study. FWHMs measured with $\theta = 90^\circ$ for the double-cone and single-cone pinholes were 4.63 mm and 7.98 mm, respectively. The difference in resolution is most pronounced when $\theta = 90^\circ$. The theoretical FWHMs calculated at the detector plane were 3.10 mm and 7.15 mm for the double-cone and single-cone pinholes respectively. This compares well with the simulation results.

Figures 12(a) and 12(b) show that results from the analytical model for sensitivity are in good agreement with the simulation results for both geometries. However, as the source moves away from the centre of the pinholes, the analytical model begins to underestimate the penetrative sensitivity. This error is due to the assumption used in both models that all second order terms are negligible. In addition, the analytical

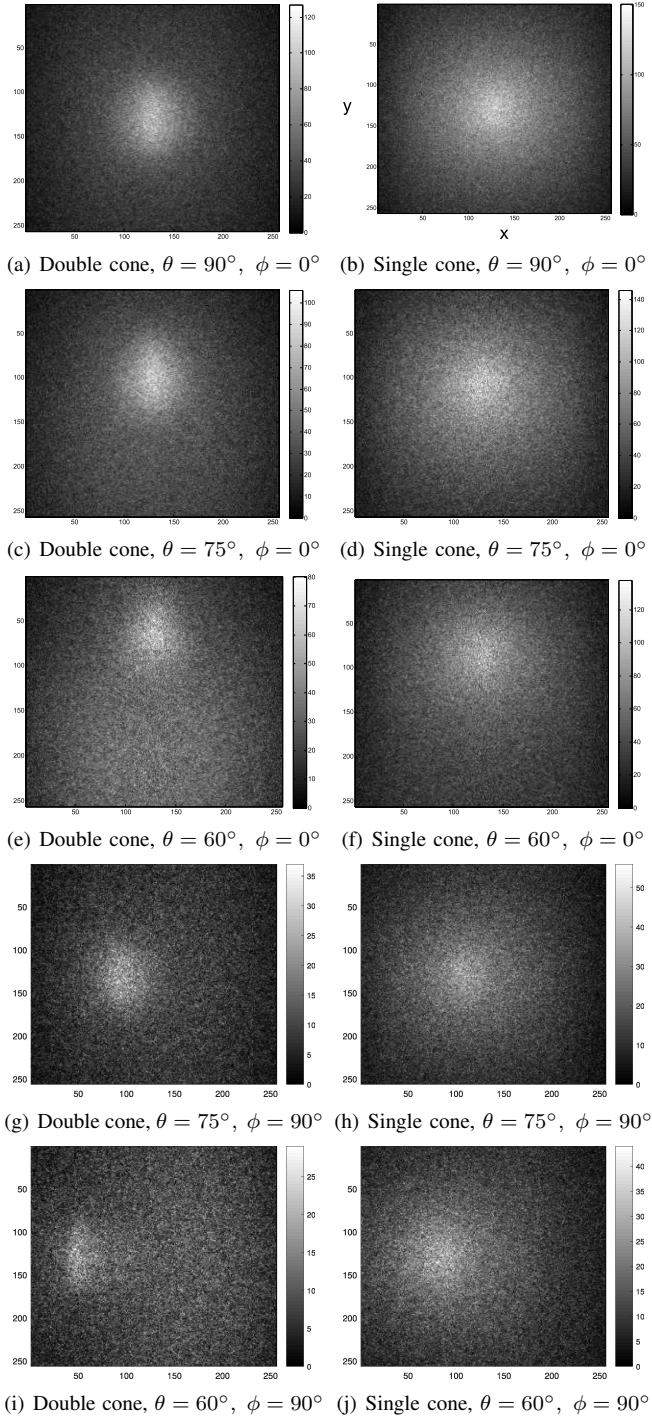


Fig. 9. Monte Carlo simulation of the projection of an image of a ^{192}Ir source located at $(\theta, \phi) = (60^\circ, 0^\circ)$, $(60^\circ, 90^\circ)$, $(75^\circ, 0^\circ)$, $(75^\circ, 90^\circ)$ and $(90^\circ, 0^\circ)$ passing through double-cone and single-cone pinholes onto a single 256×256 pixel detector array.

models assume that photons cannot penetrate the full thickness of the collimator. However, this is not the case in practice, as approximately 20% of the gamma photons from an ^{192}Ir source incident on a 4 mm thick tungsten slab will penetrate the collimator and reach the detector surface. The discrepancy between the models becomes larger as $\theta \rightarrow 0^\circ$, since the ratio of the number of photons traversing the pinhole to the number penetrating the collimator body decreases as θ decreases.

V. CONCLUSION

An analytical model describing the sensitivity of a single-cone pinhole has been derived and compared to an equivalent double-cone geometry. The theoretical FWHM of the PRFs of the double-cone and single-cone pinhole PRFs were calculated based on previously published analytical resolution models, and were shown to be in good agreement with results obtained from Monte Carlo simulations using a realistic source model.

The penetrative sensitivity of the double-cone pinhole decreases more rapidly with horizontal displacement in comparison with the single-cone geometry. The greater penetrative sensitivity of the single-cone pinhole results in a larger direct photon flux on the detector, particularly for larger horizontal displacements.

The difference between the CoM of the projection from the Monte Carlo simulations and the true projected centre of the source was found to be similar for both pinhole geometries when the source was entirely contained within the FoV; however, a much greater difference was observed for the single-cone pinhole at the very edge of the field of view. Since the CoM of the projection will be used to estimate the projection of the centre of the source in *HDR BrachyView*, the double-cone pinhole will therefore enable more accurate source tracking in *HDR BrachyView*.

Therefore, based on the analytical and simulation results for resolution, sensitivity and the accuracy of the estimated projected centre of the source, the double-cone pinhole collimator geometry is the most suitable choice for the *HDR BrachyView* probe.

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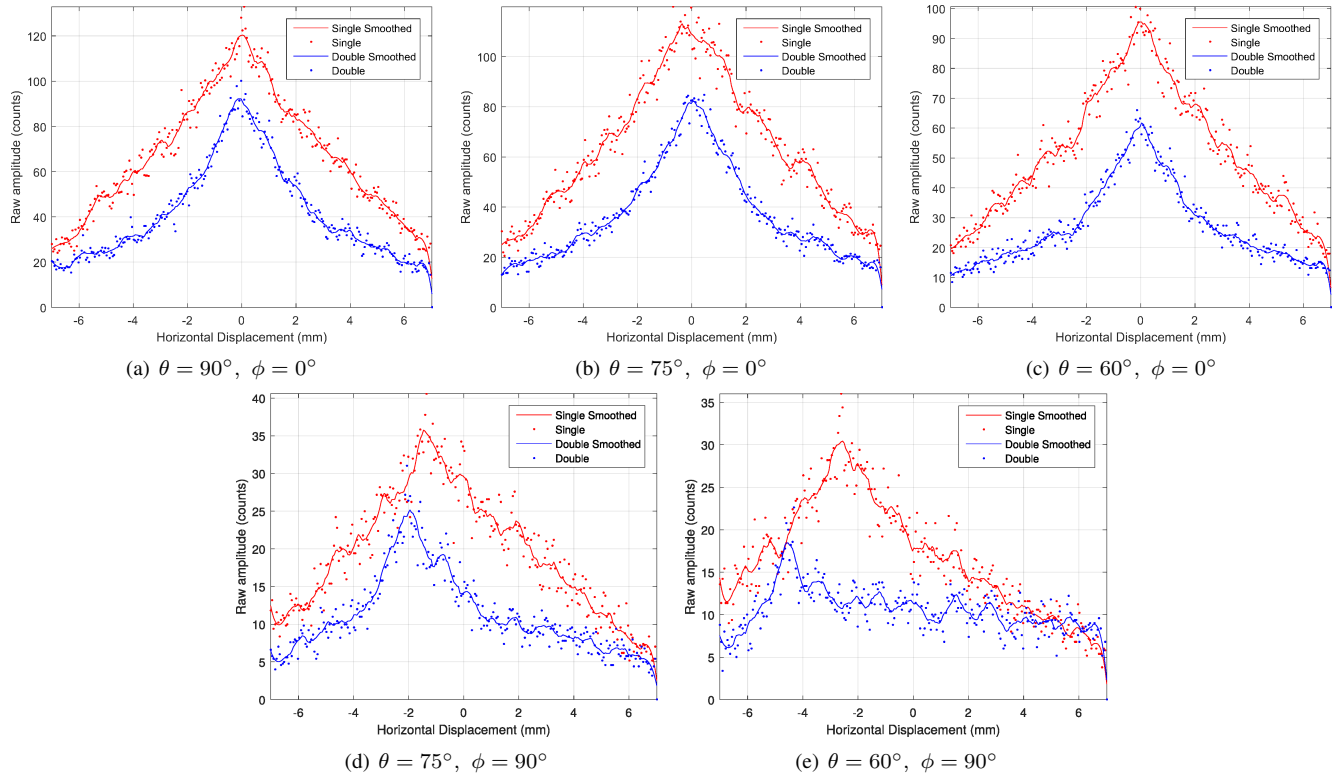


Fig. 10. PRFs obtained from simulations of double-cone and single-cone pinhole geometries for the five source positions. PRFs are measured across the centre of the projection image parallel to the x -axis and smoothed using a Savitsky-Golay filter.

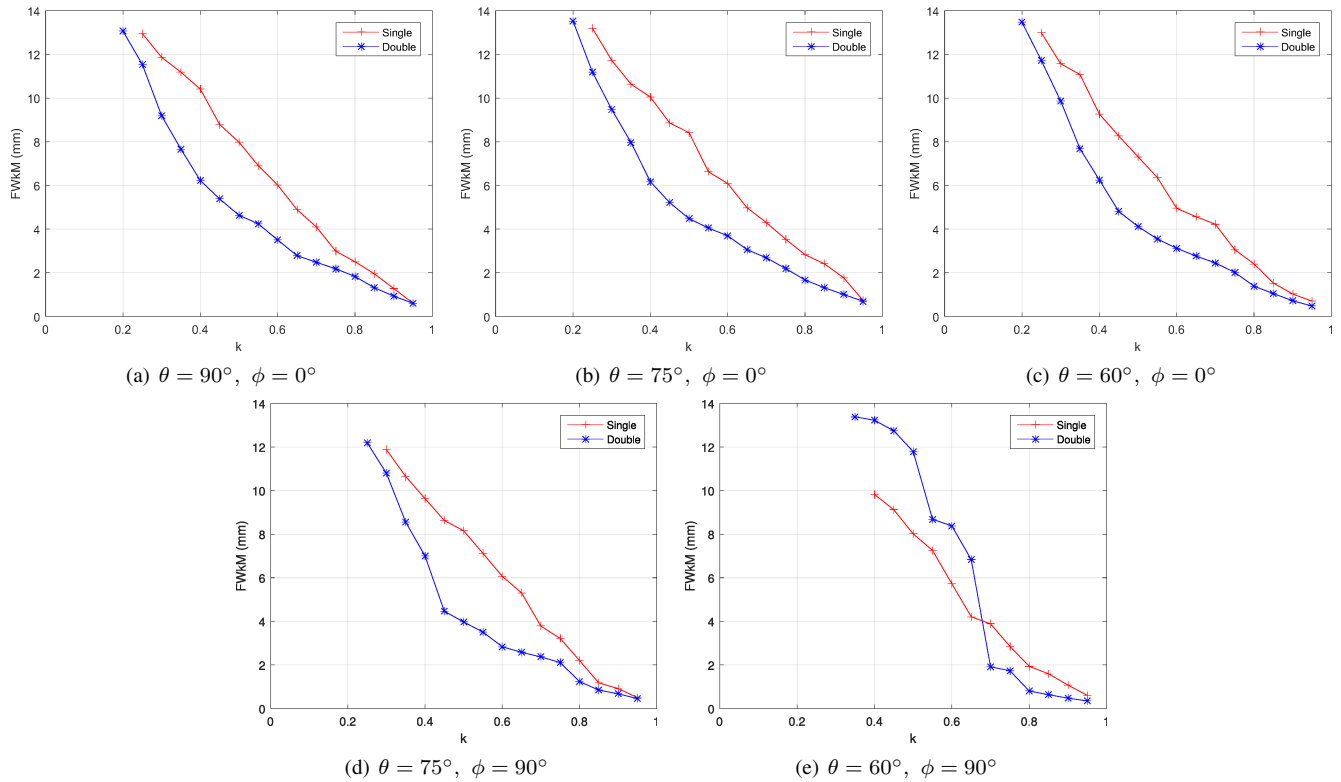


Fig. 11. FWkM calculated for k between 0.2 (and 0.25 for single-cone) and 0.95 for single-cone and double-cone pinhole geometries, computed from the simulated PRF profiles for $(\theta, \phi) = (60^\circ, 0^\circ), (60^\circ, 90^\circ), (75^\circ, 0^\circ), (75^\circ, 90^\circ)$ and $(90^\circ, 0^\circ)$. For this geometry, FWkM could not be evaluated for small values of k due to the limited width of the detector.

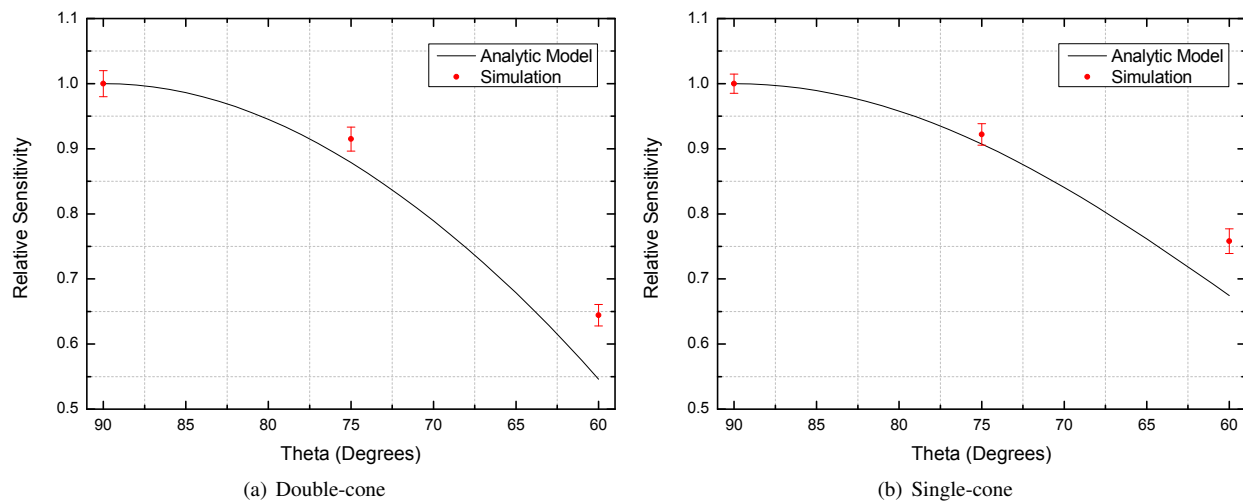


Fig. 12. Penetrative sensitivity model validation of the analytical model using Monte Carlo simulations for double-cone and single-cone pinhole geometries normalised at $\theta = 90^\circ$.

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